

FORM PTO-1390 (Modified)
(REV 11-98)

U.S. DEPARTMENT OF COMMERCE PATENT AND TRADEMARK OFFICE

ATTORNEY'S DOCKET NUMBER

TRANSMITTAL LETTER TO THE UNITED STATES
DESIGNATED/ELECTED OFFICE (DO/EO/US)
CONCERNING A FILING UNDER 35 U.S.C. 371

GJE-0004

U.S. APPLICATION NO. IF KNOWN, SEE 37 CFR

09/786499

INTERNATIONAL APPLICATION NO.
PCT/GB99/02715INTERNATIONAL FILING DATE
August 20, 1999PRIORITY DATE CLAIMED
September 3, 1998

TITLE OF INVENTION

SIGNAL PROCESSING

APPLICANT(S) FOR DO/EO/US

MICHAEL HOBSON, ET AL.

Applicant herewith submits to the United States Designated/Elected Office (DO/EO/US) the following items and other information:

1. ☒ This is a **FIRST** submission of items concerning a filing under 35 U.S.C. 371.
2. ☐ This is a **SECOND** or **SUBSEQUENT** submission of items concerning a filing under 35 U.S.C. 371.
3. ☒ This is an express request to begin national examination procedures (35 U.S.C. 371(f)) at any time rather than delay examination until the expiration of the applicable time limit set in 35 U.S.C. 371(b) and PCT Articles 22 and 39(1).
4. ☒ A proper Demand for International Preliminary Examination was made by the 19th month from the earliest claimed priority date.
5. ☒ A copy of the International Application as filed (35 U.S.C. 371 (c) (2))
 - a. ☒ is transmitted herewith (required only if not transmitted by the International Bureau).
 - b. ☐ has been transmitted by the International Bureau.
 - c. ☐ is not required, as the application was filed in the United States Receiving Office (RO/US).
6. ☐ A translation of the International Application into English (35 U.S.C. 371(c)(2)).
7. ☒ A copy of the International Search Report (PCT/ISA/210).
8. ☐ Amendments to the claims of the International Application under PCT Article 19 (35 U.S.C. 371 (c)(3))
 - a. ☐ are transmitted herewith (required only if not transmitted by the International Bureau).
 - b. ☐ have been transmitted by the International Bureau.
 - c. ☐ have not been made; however, the time limit for making such amendments has NOT expired.
 - d. ☐ have not been made and will not be made.
9. ☐ A translation of the amendments to the claims under PCT Article 19 (35 U.S.C. 371(c)(3)).
10. ☒ An oath or declaration of the inventor(s) (35 U.S.C. 371 (c)(4)).
11. ☐ A copy of the International Preliminary Examination Report (PCT/IPEA/409).
12. ☐ A translation of the annexes to the International Preliminary Examination Report under PCT Article 36 (35 U.S.C. 371 (c)(5)).

Items 13 to 20 below concern document(s) or information included:

13. ☐ An Information Disclosure Statement under 37 CFR 1.97 and 1.98.
14. ☒ An assignment document for recording. A separate cover sheet in compliance with 37 CFR 3.28 and 3.31 is included.
15. ☒ A **FIRST** preliminary amendment.
16. ☐ A **SECOND** or **SUBSEQUENT** preliminary amendment.
17. ☐ A substitute specification.
18. ☐ A change of power of attorney and/or address letter.
19. ☒ Certificate of Mailing by Express Mail
20. ☒ Other items or information:

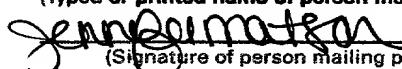
Postcard

"Express Mail" mailing label number EL71878421008Date of Deposit March 2, 2001

I hereby certify that this paper or fee is being deposited with the United States Postal Service "Express Mail Post Office to Addressee" service under 37 CFR 1.10 on the date indicated above and is addressed to the Commissioner of Patents and Trademarks, Washington, D.C. 20231.

Jennifer Matson

(Typed or printed name of person mailing paper or fee)


 (Signature of person mailing paper or fee)

U.S. APPLICATION NO. (IF KNOWN) SEE 37 CFR 1.53 <div style="font-size: 24pt; font-weight: bold; text-align: center;">097786499</div>	INTERNATIONAL APPLICATION NO. <div style="text-align: center;">PCT/GB99/02715</div>	ATTORNEY'S DOCKET NUMBER <div style="text-align: center;">GJE-0004</div>
---	--	---

21. The following fees are submitted:				CALCULATIONS PTO USE ONLY	
BASIC NATIONAL FEE (37 CFR 1.492 (a) (1) - (5)) :					
<input type="checkbox"/> Neither international preliminary examination fee (37 CFR 1.482) nor international search fee (37 CFR 1.445(a)(2)) paid to USPTO and International Search Report not prepared by the EPO or JPO \$1,000.00					
<input checked="" type="checkbox"/> International preliminary examination fee (37 CFR 1.482) not paid to USPTO but International Search Report prepared by the EPO or JPO \$860.00					
<input type="checkbox"/> International preliminary examination fee (37 CFR 1.482) not paid to USPTO but international search fee (37 CFR 1.445(a)(2)) paid to USPTO \$710.00					
<input type="checkbox"/> International preliminary examination fee paid to USPTO (37 CFR 1.482) but all claims did not satisfy provisions of PCT Article 33(1)-(4) \$690.00					
<input type="checkbox"/> International preliminary examination fee paid to USPTO (37 CFR 1.482) and all claims satisfied provisions of PCT Article 33(1)-(4) \$100.00					
ENTER APPROPRIATE BASIC FEE AMOUNT =				\$860.00	
Surcharge of \$130.00 for furnishing the oath or declaration later than <input type="checkbox"/> 20 <input type="checkbox"/> 30 months from the earliest claimed priority date (37 CFR 1.492 (e)).				\$0.00	
CLAIMS	NUMBER FILED	NUMBER EXTRA	RATE		
Total claims	16 - 20 =	0	x \$18.00	\$0.00	
Independent claims	1 - 3 =	0	x \$80.00	\$0.00	
Multiple Dependent Claims (check if applicable). <input type="checkbox"/>				\$0.00	
TOTAL OF ABOVE CALCULATIONS =				\$860.00	
Reduction of 1/2 for filing by small entity, if applicable. Verified Small Entity Statement must also be filed (Note 37 CFR 1.9, 1.27, 1.28) (check if applicable). <input type="checkbox"/>				\$0.00	
SUBTOTAL =				\$860.00	
Processing fee of \$130.00 for furnishing the English translation later than <input type="checkbox"/> 20 <input type="checkbox"/> 30 months from the earliest claimed priority date (37 CFR 1.492 (f)).				\$0.00	
TOTAL NATIONAL FEE =				\$860.00	
Fee for recording the enclosed assignment (37 CFR 1.21(h)). The assignment must be accompanied by an appropriate cover sheet (37 CFR 3.28, 3.31) (check if applicable). <input type="checkbox"/>				\$0.00	
TOTAL FEES ENCLOSED =				\$860.00	
				Amount to be: refunded	\$
				charged	\$

☒ A check in the amount of **\$860.00** to cover the above fees is enclosed.

☐ Please charge my Deposit Account No. _____ in the amount of _____ to cover the above fees.
 A duplicate copy of this sheet is enclosed.

☒ The Commissioner is hereby authorized to charge any fees which may be required, or credit any overpayment to Deposit Account No. **06-1130** A duplicate copy of this sheet is enclosed.

NOTE: Where an appropriate time limit under 37 CFR 1.494 or 1.495 has not been met, a petition to revive (37 CFR 1.137(a) or (b)) must be filed and granted to restore the application to pending status.

SEND ALL CORRESPONDENCE TO:

CANTOR COLBURN LLP
 55 Griffin Road South
 Bloomfield, CT 06002
 Telephone: 860-286-2929

SIGNATURE

Daniel F. Drexler
 NAME

P47,535
 REGISTRATION NUMBER

March 2, 2001
 DATE

Express Mail Label #EL718784210US

IN THE UNITED STATES PATENT AND TRADEMARK OFFICE

IN RE APPLICATION OF: MICHAEL HOBSON, ET AL

FOR: 35 U.S.C. §371 NATIONAL STAGE ENTRY OF PCT/GB99/02715

TITLE: SIGNAL PROCESSING

MAILED: March 2, 2001, with Certificate of Mailing by Express Mail

PRELIMINARY AMENDMENT

Box Patent Application
The Assistant Commissioner of
Patents and Trademarks
Washington, DC 02031

Sir:

Prior to the Examiner acting in the above-referenced application, please preliminary amend
the specification and claims as follows:

"Express Mail" mailing label number EL718784210US
Date of Deposit March 2, 2001
I hereby certify that this paper or fee is being deposited
with the United States Postal Service "Express Mail
Post Office to Addressee" service under 37 CFR 1.10
on the date indicated above and is addressed to the
Commissioner of Patents and Trademarks, Washington,
D.C. 20231.
Jennifer Matson
(Typed or printed name of person mailing paper or fee)
Jennifer Matson
(Signature of person mailing paper or fee)

IN THE SPECIFICATION

Please insert the following specification paragraph in re-written “clean form”. This is the first paragraph on the first page of the specification.

--TECHNICAL FIELD OF THE INVENTION

The present invention relates to the reconstruction of signals. There are many applications, such as radar, sonar, acoustic data, spectroscopy, geophysical, and image signal processing, in which it is desirable to reconstruct signals from given data.

DESCRIPTION OF THE RELATED ART--.

Please insert the following specification paragraph in re-written “clean form”. This is the fourth paragraph on the first page of the specification.

--SUMMARY OF THE INVENTION

The present invention is directed towards improving the reconstruction of signals from given data so that such reconstruction can be performed within a reduced time frame.--.

Please insert the following specification paragraph in re-written “clean form”. This is the fifth complete paragraph on the second page of the specification.

--DETAILED DESCRIPTION OF THE PREFERRED EMBODIMENT

One example of the present invention will now be described--.

IN THE CLAIMS:

Claim 4 is presented as follows in re-written clean format.

--4. (Amended) A method according to claim 1, wherein the Bayesian reconstruction employs a maximum entropy method.--

Claim 8 is presented as follows in re-written clean format.

--8. (Amended) A method according to claim 1, wherein the signal to be reconstructed is an image signal.--

Claim 10 is presented as follows in re-written clean format.

--10. (Amended) A method according to claim 1, wherein the signal to be reconstructed is a radar signal.--

Claim 11 is presented as follows in re-written clean format.

--11. (Amended) A method according to claim 1, wherein the signal to be reconstructed is an acoustic data signal.--

Claim 14 is presented as follows in re-written clean format.

--14. (Amended) A method according to claim 1, wherein the signal to be reconstructed is a signal from spectroscopy.—

Claim 15 is presented as follows in re-written clean format.

--15. (Amended) A method according to claim 1, wherein the signal is a communication signal.--

Please enter the following new claim.

--16. (Newly Added) A method according to claim 15, wherein the communication signal is a time-series signal.--

REMARKS

Applicants request entry of the above-identified amendments which, in part, reduce multiple dependencies and conform the claims and specification to U.S. practice. No new matter is being introduced by this Amendment as antecedent support is set forth in the specification and the original claims.

Entry of the amendments and prosecution on the merits is respectfully requested.

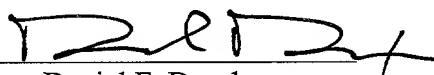
The Examiner is invited to contact Applicants' attorneys directly by telephone at the below-listed telephone number with any questions, comments or concerns, or if Applicants' attorneys can otherwise be of any assistance.

If there are any charges with respect to this Amendment or otherwise, please charge them to Deposit Account No. 06-1130 maintained by Applicants' attorneys.

Respectfully submitted,

MICHAEL HOBSON, ET AL.

CANTOR COLBURN LLP
Applicants' Attorney

By: 

Daniel F. Drexler
Registration No. P47,535
Customer No. 23413

Date: March 2, 2001
Address: 55 Griffin Road South, Bloomfield, CT 06002
Telephone: 860-286-2929

09766499.0004
T030E0 66499Z60

VERSION WITH MARKINGS TO SHOW CHANGES MADE

A marked up version of the first paragraph replaced on the first page of the specification is as follows:

“TECHNICAL FIELD OF THE INVENTION

The present invention relates to the reconstruction of signals. There are many applications, such as radar, sonar, acoustic data, spectroscopy, geophysical, and image signal processing, in which it is desirable to reconstruct signals from given data.

DESCRIPTION OF THE RELATED ART”

A marked up version of the fourth paragraph replaced on the first page of the specification is as follows:

“SUMMARY OF THE INVENTION

The present invention is directed towards improving the reconstruction of signals from given data so that such reconstruction can be performed within a reduced time frame.”

A marked up version of the fifth complete paragraph replaced on the second page of the specification is as follows:

“DETAILED DESCRIPTION OF THE PREFERRED EMBODIMENT

One example of the present invention will now be described.”

A marked up version of claim 4 follows:

Claim 4 (Amended/Marked up) A method according to [any preceding] claim 1, wherein the Bayesian reconstruction employs [the] a maximum entropy method.

A marked up version of claim 8 follows:

Claim 8. (Amended/Marked up) A method according to [any of] claim[s] 1 [to 7], [in which] wherein the signal to be reconstructed is an image signal.

A marked up version of claim 10 follows:

Claim10. (Amended/Marked up) A method according to [any of] claim[s] 1 [to 7], [in which] wherein the signal to be reconstructed is a radar signal.

A marked up version of claim 11 follows:

Claim 11. (Amended/Marked up) A method according to [any of] claim[s] 1 [to 7], [in which] wherein the signal to be reconstructed is an acoustic data signal.

A marked up version of claim 14 follows:

Claim 14. (Amended/Marked up) A method according to [any of] claim[s] 1 [to 7], [in which] wherein the signal to be reconstructed is a signal from spectroscopy.

A marked up version of claim 15 follows:

Claim 15. (Amended/Marked up) A method according to [any of] claim[s] 1 [to 7], [in which] wherein the signal is a communication signal[, such as a time-series signal].

SIGNAL PROCESSING

5 The present invention relates to the reconstruction of signals. There are many applications, such as radar, sonar, acoustic data, spectroscopy, geophysical, and image signal processing, in which it is desirable to reconstruct signals from given data.

10 In many of these situations the effect on the signals of noise and the particular characteristic of the system generating the signal are known or can be approximated using appropriate mathematical models. In these situations, Bayesian reconstruction methods have often been applied to reconstruct the signal from given data. These methods can work well. For example one Bayesian
15 reconstruction approach, known as the maximum entropy method, is known to work well. Usually, the maximum entropy method (MEM), is only be applied to the reconstruction of signals that are strictly non-negative, and which are not complex. Given this, it is generally not
20 possible to change the basis in any vector space representing the data during any reconstruction. Being unable to do this results in computationally very expensive reconstruction processes having to be employed, because of the requirement for very large calculations having an
25 extremely large number of variables to be determined.

For example, employment of such an MEM to a stack of twenty images from a microscope takes in the region of fifty minutes using a standard INTELTM PentiumTM 200MHz processor.

30 The present invention is directed towards improving the reconstruction of signals from given data so that such reconstruction can be performed within a reduced time frame.

35 According to the present invention there is provided a method of reconstructing a signal from a given set of data, with a prediction function representing a predictable

T02030 66498260

effect on the signal, and a noise function representing unpredictable noise, the method comprising the steps of:

altering the coordinate basis of the data and signal from an original coordinate basis in order to produce a prediction function having a reduced set of variables;

performing a Bayesian reconstruction capable of operation of positive, negative, and complex signal values to produce a reconstruction signal; and

converting the reconstruction signal back into the original coordinate basis to generate a signal.

The Bayesian reconstruction may be performed using a Fourier basis, or may use a wavelet basis.

The Bayesian reconstruction may employ the maximum entropy method, in which case the method may employ an evaluation parameter, α , which may be determined from a prior reconstruction, set at a fixed value, or determined during the reconstruction step.

The signal to be reconstructed may be an image signal, or may be a radar, sonar, or acoustic data signal. Alternatively, it may be a signal from spectroscopy or a geophysical signal.

By employing the method of the present invention, an example stack of 20 microscope images takes approximately 45 seconds to reconstruct using a standard INTELTM PentiumTM 200 MH² processor.

One example of the present invention will now be described.

097649-000
102000-66494260

Bayesian reconstruction methods have been applied to numerous problems in a wide variety of fields. In their standard form, however, they can be very computationally intensive, since they generally require the numerical maximisation of a complicated function of many variables.

For example, in image reconstruction problems, it is not unusual for the number of variables to be $\sim 10^6$. Furthermore, one of the most popular Bayesian reconstruction algorithms is the maximum-entropy method (MEM), which can only be applied to the reconstruction of signals that are strictly non-negative (see below). The method can, however, be extended to signals that can take both positive and negative values. We develop the MEM approach so that it can be applied to the reconstruction of signals that can take positive, negative or complex values. As a result, this enables the use of similarity transformations in the reconstruction algorithm so that calculations can be performed in an alternative "basis" this is more appropriate to the problem under consideration. Specifically, the basis is chosen so that signal is reconstructed by performing a large number of numerical maximisations of low dimensionality, rather than a single maximisation of high dimensionality. This results in a significant increase in speed. Indeed, in the example outlined below, the speed of the reconstruction algorithm is increased by a factor of about 100.

The standard Bayesian reconstruction techniques mentioned above are typically applied to a given data set $d(y)$ in order to reconstruct some underlying signal $s(x)$. Here, y denotes the space over which the data are defined and x denotes the space of the signal, which may in general be distinct from x and need not have the same number of dimensions. For example, given some data stream $d(t)$, which consists of the measured values of some quantity as a function of time t , we may wish to reconstruct the two-

dimensional spatial variation of some other quantity (or signal) $s(x,y)$.

For most measurements it is convenient (or necessary) to digitise the data and the signal (for example if either is to be stored/analyzed on a digital computer). We may therefore denote the data by the vector d with N_d components, where N_d is the number of data samples. Similarly, we denote the signal by the vector s of length N_s , where N_s is the number of points at which we wish to reconstruct the signal.

In general, we may express the data vector as some function ϕ of the signal vector, i.e.

$$d = \phi(s)$$

The function ϕ can be non-linear and specifies the effect of the measuring apparatus on the signal that we wish to reconstruct. It is customary to divide this function into the predictable effect of the measuring apparatus on the signal and the stochastic noise part due to inherent inaccuracies in the measurement process. In this case, we may write

$$d = \phi(s) + \epsilon, \quad (1)$$

Where ϕ denotes the predictable response of the apparatus to the signal and ϵ is a vector of length N_d that contains any stochastic noise contributions to the data.

The Bayesian approach to reconstructing the signal is to calculate the estimator \hat{s} that maximises the posterior probability $\Pr(s|d)$. This is given by Bayes' theorem as

$$\Pr(s|d) = \frac{\Pr(d|s) \Pr(s)}{\Pr(d)},$$

where $\Pr(d|s)$ is the likelihood of obtaining the data given the signal, $\Pr(s)$ is the prior probability, and the evidence $\Pr(d)$ can be considered merely as a normalisation constant. Thus, in order to obtain the (Bayesian estimator of the signal vector, we must maximise the product the product $\Pr(d|s) P(s)$ of the

likelihood function and the prior. A thorough discussion of Bayesian analysis techniques is given by Sivia (1996).

The likelihood function describes the statistics of noise contribution ϵ to the data. This function may take any form appropriate to the noise statistics. It is convenient to define the log-likelihood function $L(s) = \ln[\Pr(d|s)]$ so that the likelihood function may be written as $\Pr(d|s) = \exp[L(s)]$. As an example, if the noise on the data is Gaussian-distributed and described by the noise covariance matrix N , then the likelihood function takes the form

$$\begin{aligned} \Pr(d|s) &\propto \exp\left[-\frac{1}{2}\epsilon^T N^{-1}\epsilon\right] \\ &\propto \exp\left[-\frac{1}{2}(d - \Phi(s))^T N^{-1}(d - \Phi(s))\right], \end{aligned} \quad (2)$$

where in the second line we have used (1). In this case, the log-likelihood function is simply minus one half of the standard χ^2 misfit statistic, i.e.

$$L(s) = -\frac{1}{2}\chi^2(s).$$

The prior distribution $\Pr(s)$ codifies our knowledge of the underlying signal before acquiring the data. If we have some advance knowledge of the statistical properties of the signal then this is contained in the prior. For example, if we assume the signal to be described by a Gaussian random field with a covariance matrix C , then the prior takes the form

$$\Pr(s) \propto \exp\left(-\frac{1}{2}s^T C^{-1}s\right).$$

Indeed, if the prior is assumed to have this form and the likelihood is also Gaussian, as in (2), then the Bayesian estimator \hat{S} is obtained by maximising their product is identical to the standard Wiener filter solution. An introduction to the Wiener filter technique is given by Press et al (1994).

It is clear, however, that although the noise contribution to the data may often be Gaussian-distributed, the assumption of a Gaussian form for the prior is not valid for a general signal. If the joint probability distribution of the elements of the signal vector is known then it should be used as the prior. This is almost always impossible, however, and we instead investigate the assignment of a prior applicable to general signals that is based on information-theoretic considerations alone. Using very general notions of subset independence, coordinate invariance and system independence, it may be shown that the prior probability $\Pr(s)$ should take the form

$$\Pr(s) \propto \exp[\alpha S(s, m)], \quad (3)$$

Where the dimensional constant α depends on the scaling of the problem and may be considered as a regularising parameter, and m is a model to which the Bayesian reconstruction defaults in the absence of any data and is usually set to a small constant value. The function $S(s, m)$ is the cross-entropy of the signal and model vectors and is given by

$$S(s, m) = \sum_{n=1}^{N_s} \left[s_n - m_n - s_n \ln \left(\frac{s_n}{m_n} \right) \right], \quad (4)$$

Where N_s is the length of the (digitised) signal vector. A derivation of this result is given by Skilling (1988). By combining the entropic prior with the likelihood function, the Bayesian estimator of the signal is found by maximising with respect to s the posterior probability, which now takes the form

$$\Pr(s|d) \propto \exp[L(s)] \exp[\alpha S(s, m)] = \exp[L(s) + \alpha S(s, m)].$$

Thus, maximising this probability distribution is equivalent to maximising the function

$$F(s) = L(s) + \alpha S(s, m), \quad (5)$$

and this forms the basis of the maximum entropy method (MEM).

5

The maximum-entropy method has been applied to a wide range of signal reconstruction problems. In its standard form, however, it can be very computationally intensive. The function $F(s)$ is in general a complicated function of the components s_n of the signal vector and so a numerical maximisation of the $F(s)$ must be performed over this N_s -dimensional space. It is not unusual for N_s to be of the order $N_s \sim 10^6$, particularly in image reconstruction problems. Moreover, the standard MEM approach is only applicable to signals that are strictly non-negative, as is clear from the presence of the logarithmic term in the expression (4) for the entropy.

Nevertheless, it is possible to extend the MEM so that it can be applied to the reconstruction of signals that can take both positive and negative values. The definition of the entropy for positive/negative signals with certain special properties was first presented by Gull & Skilling (1990). The generalisation to arbitrary positive/negative signals and the derivation of the prior probability in this case is given by Hobson & Lasenby (1998). It is found that the prior has the same form as given (3) but the expression for the entropy $S(s, m)$ must be modified. The central idea is to express the general (positive/negative) signal vector s as the difference of two vectors u and v containing only strictly non-negative distributions, i.e.

$$s = u - v$$

By applying continuity constraints on the entropy functional it is possible that the expression for the entropy for the positive/negative signal s is given by

$$S(s, m_u, m_v) = \sum_{n=1}^{N_s} \left\{ \psi_n - (m_u)_n - (m_v)_n - s_n \ln \left[\frac{\psi_n + s_n}{2(m_u)_n} \right] \right\} \quad (6)$$

Where m_u and m_v are separate models for u and v respectively, and where $\psi_n = [s_n^2 + 4(M_u)_n(M_v)_n]^{1/2}$. We cannot hope to replace the models m_u and m_v by a single positive/negative model m_s (say), since such a distribution could no longer be considered as an integration measure. Nevertheless, we can still consider the difference $m_u - m_v$ as the model for the signal s . We note that the form of the positive/negative entropy derived by Gull & Skilling (1990) requires $m_u = m_v$.

Given the entropic prior for general positive/negative signals, it is then straightforward to define the prior for complex signals simply by applying the above analysis to the real and imaginary parts separately. In this case the models M_u and M_v are also taken to be complex. The real and imaging parts of m_u are the models for the positive portions of the real and imaginary parts of s respectively. Similarly, the real and imaginary parts of m_v are the models for the negative portions of the real and imaginary parts of the image. The total entropy of the complex signal is then obtained by evaluating the sum (6) using first the real parts and then the imaginary parts of s , m_u and m_v and adding the results.

The ability to reconstruct positive/negative and complex distributions using the MEM approach has profound consequences for greatly improving the both the speed and accuracy of the MEM technique. These improvements are based on the idea of making a change of basis in both the signal and data spaces and performing a Bayesian reconstruction in this new basis. With an appropriate choice of the new bases, it is possible to speed up significantly the calculation of the reconstruction, which can then easily be rotated back into the original basis in signal space to obtain the final reconstruction of the signal. For example, the ability to reconstruct

complex signals allows us to perform reconstructions in the Fourier basis of complex exponentials, which greatly reduces the computational complexity of de-blurring images that have been convolved with a spatially varying point-spread function (see the example below).

In order to understand how a general change of basis is performed we must first remind ourselves of some basic results in linear algebra and vector (see e.g. Riley, Hobson & Bence 1997). Suppose there exists a set of linearly independent vectors $e^{(n)}$ ($n=1, \dots, N_s$), that form a complete basis for the N_s -dimensional space of the signal vector. We may then write the signal vector as a weighted sum of these vectors. Formally, if we take $e^{(n)}$ to be the column vector with unity as the n th element and zeros elsewhere, then we may write the signal vector as

$$s = \sum_{n=1}^{N_s} s_n e^{(n)}.$$

Thus we see that in order to reconstruct the signal vector, we are in fact reconstructing its coefficients in this trivial basis. We can, however, equally well expand the signal vector in terms of any other linearly independent set of vectors $e'^{(n)}$ ($n=1, \dots, N_s$) such that

$$s = \sum_{n=1}^{N_s} s'_n e'^{(n)}.$$

We may perform a similar procedure in the N_d -dimensional data space, which is in general distinct from the signal space. If we consider the trivial basis vectors $f^{(n)}$ ($n=1, \dots, N_d$) in this space, with unity as the n th elements and zeros elsewhere, then the data vector is given by

$$d = \sum_{n=1}^{N_d} d_n f^{(n)}.$$

On performing change of basis in data space to some other basis $f'^{(n)}$, this becomes

$$d = \sum_{n=1}^{N_d} d'_n f'^{(n)}.$$

Since the noise vector ϵ also belongs to the data space a similar change of basis can apply to it, such that

$$\epsilon = \sum_{n=1}^{N_d} \epsilon_n f^{(n)} = \sum_{n=1}^{N_d} \epsilon'_n f'^{(n)}.$$

5

It is clear that, even if the element s_n of the signal vector in the original basis were strictly non-negative, the elements s'_n in the new basis will in general take both positive and negative values.

10 Furthermore, in the case where the new basis vectors have complex components, the coefficients s'_n may themselves be complex. Hence it is the extension of the MEM technique to the reconstruction of such quantities that allows this approach to be taken.

15 Once we have performed the changes of basis in the data and signal spaces, we denote the vectors with components s'_n by s' and we similarly define the vectors d' and ϵ' as those containing the elements d'_n and ϵ'_n respectively. In the signal space we can relate the two bases $e^{(n)}$ and $e'^{(n)}$ ($n=1, \dots, N_s$) by

$$e'^{(n)} = \sum_{i=1}^{N_s} U_{in} e^{(i)}$$

where U_{in} is the i th component of $e'^{(n)}$ with respect to the original (unprimed) basis. The vector s' and s are then related by

$$s = Us' \quad (7)$$

Similar results hold for the bases $f^{(n)}$ and $f'^{(n)}$ ($n = 1, \dots, N_d$) in data space, such that

$$d = Vd' \quad (8)$$

30 Where the element V_{in} is the i th component of $f'^{(n)}$ with respect to the unprimed basis. A similar expression exists relating the noise vectors ϵ' and ϵ . Substituting (7) and (8) and (1), we then obtain

$$35 \quad d' = \Phi'(s') + \epsilon', \quad (9)$$

Where ϕ' is a new function relating the signal and data vectors in the new basis.

Clearly, our aim is to choose the new bases in the data and signal spaces in order that the relationship (9) takes the simplest form. More formally, we wish to perform similarity transformations in the data and signal spaces that partition each space into numerous (quasi-) disjoint subspaces of much lower dimensionality. In such bases, we may then calculate the estimate \hat{s}' of the rotated signal vector by performing numerical maximisations in each subspace separately. Thus, we replace a single maximisation over the N_s -dimensional signal space in the original basis by numerous low-dimensionality maximisations over each subspace in the new basis. This leads to a considerable increase in the speed with which the reconstruction can be performed. Then, having calculated the Bayesian reconstruction \hat{s}' in the new basis, the required signal reconstruction \hat{s} can be obtained by rotating back to the original signal-space basis. We reiterate that, since the elements S_m in the new basis can in general take positive, negative or even complex values, it is the extension of the MEM technique to the reconstruction of such quantities that allows this approach to be taken.

As an example, let us consider the application of the above Bayesian reconstruction technique to the deconvolution of images that have been blurred by a spatially-invariant point-spread function (PSF) and that may also contain some noise contribution. For simplicity, we will assume that the de-blurred reconstruction is produced on the same pixelisation as the blurred image, although this is clearly not required by the technique in general. In this simple case, the data and signal spaces coincide.

It is well known that the convolution of an underlying image with a spatially invariant PSF is equivalent to multiplying together their Fourier

transforms and then performing an inverse Fourier transform. Therefore, in the Fourier domain, each Fourier mode can be considered independently of the others. This suggests that we should perform the Bayesian reconstruction in the Fourier basis, such that

$$s'_n = \sum_{m=1}^{N_s} \exp(-in\pi(m-1)/N_s) s_m.$$

With a similar expression relating the components of the data vectors d' and d and the noise vectors ϵ and ϵ' (Since the data and signal spaces coincide). Thus, in this case, the N_s -dimensional signal (and data) space has been partitioned into N_s separate disjoint spaces (i.e. one for each Fourier mode).

Now for each value of n (or Fourier mode), we may consider the elements d'_n , s'_n and ϵ'_n independently of those for other values of n . This leads to a substantial decrease in the CPU time required to de-blur a given image. For simplicity, at our chosen Fourier mode we denote d'_n , s'_n and ϵ'_n by d' , s' and ϵ' respectively. The quantity d' is given simply by the Fourier coefficient of the true underlying image, or signal s' , multiplied by the Fourier coefficient of the PSF, or response R . In addition, a noise contribution, ϵ' , in the Fourier domain may also be present. If no instrumental errors are expected from a given apparatus, it is still possible to introduce "noise" by, for example, digitising an image in order to store it on a computer. Thus the data value is given by

$$d' = Rs' + \epsilon' \quad (10)$$

Since we are performing the reconstruction in the Fourier basis, the noise on each Fourier mode will contain contributions from a wide range of scales. Therefore, provided the noise on the image is distributed in a statistically-homogeneous manner, we would expect from the central limit theorem that the noise in the Fourier domain is described reasonably well by a Gaussian

distribution. Therefore, the likelihood function is given by

$$\Pr(d'|s') \propto \exp(-|d' - Rs'|^2/\sigma^2),$$

5 where $\sigma^2 = \langle \epsilon' \epsilon'^* \rangle$ is the variance of the noise contribution at the particular Fourier mode under consideration. From (6), the entropy $S(s', m)$ of this complex "image" may be shown to be given by (where we have set $m_u = m_v = m$)

$$10 \quad S(s, m) = \Re(\psi) - 2\Re(m) - \Re(s') \ln \left[\frac{\Re(\psi + s')}{2\Re(m)} \right] + \Im(\psi) - 2\Im(m) - \Im(s') \ln \left[\frac{\Im(\psi) + \Im(s')}{2\Im(m)} \right],$$

where the \Re and \Im denote the real or imaginary part respectively of a complex number; also $\Re(\psi) = [\Re(s')^2 + 4\Re(m)^2]^{1/2}$ and a similar expression exists for $\Im(\psi)$.

15 Using the above expression for the likelihood and prior, and assuming a particular value for the regularising parameter α in (5), it is then possible numerically to maximise the posterior probability to obtain the estimator \hat{s}' of the signal vector at each Fourier mode independently. Once these estimators have been calculated for all the Fourier modes, we simply perform an inverse Fourier transform to recover the de-blurred image, i.e.

$$25 \quad \hat{s}_n = \frac{1}{N_s} \sum_{m=1}^{N_s} \exp(+i\pi n(m-1)/N_s) \hat{s}'_m.$$

The value of α used in the reconstruction algorithm may be set in three different ways. Firstly, α may be set such that the misfit statistic χ^2 , between the observed data and that predicted from the reconstruction, is equal to its expectation value, i.e. the number of data points to be fitted. This choice is usually referred to as "historic" MEM. Alternatively, it is possible to determine the appropriate value for α in a fully Bayesian manner (Skilling 1989) by simply treating it as another parameter in our hypothesis space. This is the recommended choice and is usually referred to as

"classic" MEM. Finally, the simplest option is to fix
a in advance to some value. This option is unlikely
to yield optimal results. It can, however, be used to
obtain a quick solution if the historic or classic value
5 for a has already been determined for a particular
problem on a previous occasion.

The above technique has been applied to several
different data sets in which an image has been convolved
with a spatially-invariant point-spread function. For
10 example, the "classic" de-blurring of a microscope image
of a section through a pollen grain. The section has
dimensions 128 x 128 and is taken from a three
dimensional "stack" of 20 such images. The original stack
had been blurred by a spatially invariant three
15 dimensional PSF and the de-blurred reconstruction of the
entire stack required approximately 45 seconds on an
Intel Pentium 200 MHz processor. A standard MEM
algorithm, which does not use the similarity
transformation technique was also applied to this stack
20 of images. This produced reconstructions of a similar
quality to those obtained using the invention, but
required approximately 50 minutes CPU time on the same
machine.

Similar gains in speed can be obtained by expanding
25 the signal in different bases appropriate to the given
problem, so long as the correlation matrix of the
resulting coefficients of the data, signal and noise
vectors in the new bases is relatively sparse. For
example, similar results may be obtained by
30 reconstructing the coefficients in a wavelet expansion
(Daubechie 1992) of the signal as opposed to the Fourier
expansion used above. This case has the advantage that
the coefficients are always real. Furthermore, the
scaling/translation properties of the wavelet transform
35 allow automatic multi-resolution reconstructions of the
signal vector.

Clearly, the general method outlined above can be applied to numerous different reconstruction problems of arbitrary dimensionality. Examples include the analysis of acoustic data, radar, underwater sonar, spectroscopy, geophysical data, oil exploration and medical imaging. In addition to spatial dimensions, additional dimensions such as time, spectral behavior and polarisation are also easily accommodated.

CLAIMS

1. A method of reconstructing a signal from a given set of data, with a prediction function representing a predictable effect on the signal, and a noise function representing unpredictable noise, the method comprising the steps of:

altering the coordinate basis of the data and signal from an original coordinate basis in order to produce a prediction function having a reduced set of variables;

performing a Bayesian reconstruction capable of operation of positive, negative, and complex signal values to produce a reconstruction signal; and

converting the reconstruction signal back into the original coordinate basis to generate a signal.

2. A method according to claim 1, wherein the Bayesian reconstruction is performed using a Fourier basis.

3. A method according to claim 1, wherein the Bayesian reconstruction is performed using a wavelet basis.

4. A method according to any preceding claim, wherein the Bayesian reconstruction employs the maximum entropy method.

5. A method according to claim 4, employing an evaluation parameter, α , which is determined from a prior reconstruction.

6. A method according to claim 4, employing an evaluation parameter, α , which is set at a fixed value.

7. A method according to claim 4, employing an evaluation parameter, α , which is determined during the reconstruction step.

8. A method according to any of claims 1 to 7, in which the signal to be reconstructed is an image signal.

5 9. A method according to claim 8, wherein the image signal is a medical image signal.

10. A method according to any of claims 1 to 7, in which the signal to be reconstructed is a radar signal.

10 11. A method according to any of claims 1 to 7, in which the signal to be reconstructed is an acoustic data signal.

15 12. A method according to claim 11, wherein the acoustic data signal is an underwater sonar signal.

13. A method according to claim 11, wherein the acoustic data signal is a geophysical data signal.

20 14. A method according to any of claims 1 to 7, in which the signal to be reconstructed is a signal from spectroscopy.

25 15. A method according to any one of claims 1 to 7, in which the signal is a communication signal, such as a time-series signal.

102000-66498/50

DECLARATION AND POWER OF ATTORNEY

As a below-named inventor, I hereby declare that my residence, post office address and citizenship are as stated below next to my name; I believe I am the original, first and sole inventor (if only one name is listed below) or an original, first and joint inventor (if plural names are listed below) of subject matter which is claimed and for which a patent is sought on an invention entitled SIGNAL PROCESSING

the specification of which ☒ is attached hereto or

☐ was filed on 20 AUG 1999 as United States Application Number or PCT International Application Number PCT/GB99/02715 and was amended on (if applicable)

I hereby state that I have reviewed and understand the contents of the above identified specification, including the claims, as amended by any amendment referred to above. I acknowledge the duty to disclose information which is material to patentability as defined in 37 CFR 1.56. I hereby claim foreign priority benefits under 35 U.S.C. 119(a)-(d) or 365(b) of any foreign application(s) for patent or inventor's certificate, or 365(a) of any PCT international application which designated at least one country other than the United States of America, listed below and have also identified below, by checking the box, any foreign application for a patent or inventor's certificate, or PCT international application having a filing date before that of the application on which priority is claimed:

Prior Foreign Application Number(s)	Country	Foreign Filing Date	Priority Not Claimed	Certified Copy Attached?	
				YES	NO
98307088.9	EP	03 SEP 1998	<input type="checkbox"/>	<input type="checkbox"/>	<input type="checkbox"/>
			<input type="checkbox"/>	<input type="checkbox"/>	<input type="checkbox"/>
			<input type="checkbox"/>	<input type="checkbox"/>	<input type="checkbox"/>

As a named inventor, I hereby appoint the following registered practitioner(s) to prosecute this application and to transact all business in the Patent and Trademark Office connected therewith: Michael A. Cantor 31,152; Philmore H. Colburn II 35,101; Keith J. Murphy 33,979; Leah M. Reimer 39,341; David A. Fox 38,807; Edward J. Ellis 40,389; Michael J. Rye 34,422; William J. Cass 41,659; Pamela J. Curbelo 34,676; Andrew Ryan 43,070; James F. McLaughlin 38,048; Gerow D. Brill 34,554; David S. Fishman 19,758; Robert J. Feltovic 27,710; Juan C. Villar 34,271; Herbert M. Bedingfield, Jr. P44530; Timothy J. Olson 42,962



Direct all correspondence to:
55 Griffin Road South
Bloomfield
CT 06002
United States of America

09/06/99 030201

I hereby declare that all statements made herein of my own knowledge are true and that all statements made on information and belief are believed to be true; and further that these statements were made with the knowledge that willful false statements and the like so made are punishable by fine or imprisonment, or both, under 18 U.S.C 1001 and that such willful false statements may jeopardise the validity of the application or any patent issued thereon.

1-00

Full name of sole or
First Inventor

Michael HOBSON

Inventor's signature



Residence address

Cambridge, United Kingdom GBX

Post Office address

c/o Cavendish Laboratory, University of Cambridge, Madingley
Road, Cambridge CB3 0HE, United Kingdom

Country of Citizenship

United Kingdom ✓

Date of signature

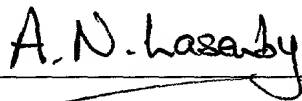
25/1/01

2-00

Full name of
Second Inventor

Anthony LASENBY

Inventor's signature



Residence address

Cambridge, United Kingdom GBX

Post Office address

c/o Cavendish Laboratory, University of Cambridge, Madingley
Road, Cambridge CB3 0HE, United Kingdom

Country of Citizenship

United Kingdom ✓

Date of signature

25th Jan 2001